

A Wavelet Based Alternative Iteration Method for the Orientation Refinement of Cryo-Electron Microscopy 3D Reconstruction

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Received March 25, 2014; revised March 6, 2015; published online May 15, 2015

Abstract. Cryo-electron microscopy (cryo-EM) single particle method (SPM) reconstructs the three-dimensional (3D) density map of biological macromolecules using 2D particle images with estimated orientations. The estimated orientations have errors which result in the decrease in resolution of the reconstructed map. We propose a wavelet orthonormal bases based iteration method by refining alternatively the orientations and the map using Levenberg–Marquardt algorithm and soft-thresholding, respectively. The convergence analysis of the proposed algorithm is provided and numerical experiments for simulated particle images show its good performance.

Keywords: alternating-direction method, convergence analysis, inverse problem, nonlinear least squares, Haar wavelet.

AMS Subject Classification: 68U10; 65J22; 65T60; 94A08; 90C90.

1 Introduction

In the past few decades, with the advance in the electron microscopes, specimen preparation methods and image processing techniques, cryo-EM techniques [6,8,12,13,17,24] have become indispensable tools for determining the 3D structures of biological macromolecules, macromolecular complexes and cells. Among all computerized techniques used in the cryo-EM technique, the SPM is one of the most popular ones. The image processing in the SPM includes image alignment and classification; image filtering and contrast transfer function correction; and 3D reconstruction (see [13,16,17,20,24] for more details). These modules are integrated in an iterative framework to iteratively refine the 3D map using the projection matching method [23].

The purpose of this paper is to develop a new algorithm to refine the reconstructed maps of cryo-EM SPM so as to obtain better resolutions. The basis principle of cryo-EM SPM 3D reconstruction lies in the 3D X-ray transform. Let $\mathbf{x} - \mathbf{y} - \mathbf{z}$ be the global coordinate system and (θ, ϕ, ψ) be three Euler angles, then the rotation matrix according to the Euler angles using $\mathbf{z} - \mathbf{y} - \mathbf{z}$ convention is defined as

$$R = (\mathbf{e}_1, \mathbf{e}_2, \mathbf{d})^\top := \begin{pmatrix} \cos \theta \cos \phi \cos \psi - \sin \theta \sin \psi & \sin \theta \cos \phi \cos \psi + \cos \theta \sin \psi & -\sin \phi \cos \psi \\ -\cos \theta \cos \phi \sin \psi - \sin \theta \cos \psi & -\sin \theta \cos \phi \sin \psi + \cos \theta \cos \psi & \sin \phi \sin \psi \\ \cos \theta \sin \phi & \sin \theta \sin \phi & \cos \phi \end{pmatrix},$$

where $\mathbf{e}_1 - \mathbf{e}_2 - \mathbf{d}$ defines the new local coordinate system after rotation, and $\mathbf{d} = (\cos \theta \sin \phi, \sin \theta \sin \phi, \cos \phi)^\top \in \mathbb{S}^2$ is the projection direction vector on the unit sphere \mathbb{S}^2 . The $\mathbf{z} - \mathbf{y} - \mathbf{z}$ convention defines the rotation matrix R by first rotating around the original z axis, then rotating around the new y axis, and finally rotating around the new z axis. The 3D X-ray transform (projection) \mathcal{P} and back-projection \mathcal{P}^* of function $f : \mathbb{R}^3 \mapsto \mathbb{R}$ along the direction \mathbf{d} are defined as

$$g(\mathbf{d}, x, y) = \mathcal{P}(\theta, \phi, \psi, x, y) := \int_{\mathbb{R}} f(x\mathbf{e}_1 + y\mathbf{e}_2 + t\mathbf{d})dt$$

and

$$(\mathcal{P}^*g)(\mathbf{x}) := \int_{\mathbb{S}^2} g(\mathbf{d}, \langle \mathbf{x}, \mathbf{e}_1 \rangle, \langle \mathbf{x}, \mathbf{e}_2 \rangle) d\mathbf{d},$$

respectively.

For every orientation (θ, ϕ, ψ) , a 2D particle image g , is imaged using transmission electron microscope, which can be described as a group of 3D X-ray transform for that orientation (θ, ϕ, ψ) . The cryo-EM SPM imaging can produce many particles images, each being a 2D projection of one biological macromolecule with a randomly produced orientation (θ, ϕ, ψ) . For SPM, all the macromolecules are identical, hence we can obtain many projections of the macromolecule with different orientations. The orientations can then be estimated using common-line based methods [5, 6, 14, 16] and thereafter be used to reconstruct an initial map. Since these particle images are picked up from the original micrographs, the centers of the particles usually deviate from the images' centers. Therefore, translational alignments among these particles should be performed before 3D reconstruction. Totally, we need five parameters $(\theta, \phi, \psi, \delta_x, \delta_y)$ in order to do reconstruction. As a result, we need to refine the five parameters for every particle image during the projection matching process. In this paper, we focus on the refinement of the three Euler angles, the proposed algorithm can be easily extended to refine all the five parameters.

The projection matching refinement methods, first proposed in [23], minimize the difference between projections and particle images. The most common algorithm of the projection matching refinement methods starts from a coarse initial angular increment (the second Euler angle ϕ), obtaining quasi-even distributions of projection directions on the unit sphere \mathbb{S}^2 . Then it calculates

the projection images using these directions. After that, it computes the similarity between every projection and particle image using Euclidean distance or cross-correlation in order to find the best matched projection for every particle image. The five parameters of the particle image then can be refined according to the best matched projection. After that, a new map is reconstructed using the particle images with refined parameters. The new map is utilized to perform new projection matching with a finer angular increment. The algorithm has been realized in some cryo-EM softwares, including EMAN [21] and Xmipp [25]. Another two refinement algorithms, one developed in the software package FREALIGN [15], using the Powell optimization algorithm, the other published in [18], utilizing the Nelder-Mead simplex minimization algorithm [22], both maximize the correlation coefficients in the Fourier space.

One of the main obstacles in the cryo-EM SPM image processing is the extremely low SNR of the particles, which results in the errors in the estimation of orientations. Hence, the main task of the orientation refinement is to overcome the affect of the noise as much as possible so as to reduce the errors of the orientations. Recently, the development of the wavelet based methods that find sparse solutions by minimizing ℓ_1 -norm of wavelet orthonormal bases or wavelet tight frame coefficients has obtained successful applications in the image restorations [2, 3, 4, 9, 10, 11] and cryo-EM SPM 3D reconstruction [19]. That motivates us to involve this idea in the refinement of cryo-EM SPM map. In this paper, we explore the wavelet orthonormal bases for its convenience in the theoretical analysis.

2 Orthonormal Wavelet Based Alternative Iteration Method

The proposed algorithm utilizes the sparse approximation of the 3D density map under the wavelet orthonormal bases and performs the orientation refinement and 3D reconstruction alternatively. In order to do 3D reconstruction, we need to compute the discretized X-ray transform and back-projection.

Let $f \in \mathbb{R}^{n^3}$ denote the vector of the 3D density map with dimension $n \times n \times n$, $g_i \in \mathbb{R}^{n^2}$ ($i = 1, \dots, m$) be the measured 2D particle images. Matrix $P_i \in \mathbb{R}^{n^2 \times n^3}$ is the discretized form of the group of 3D X-ray transforms \mathcal{P} for the orientation $(\theta_i, \phi_i, \psi_i)$ and correspondingly $[P_1^\top, \dots, P_m^\top]$ is the discretized form of the back-projection operator \mathcal{P}^* . Let

$$A = [P_1^\top, \dots, P_m^\top]^\top, \quad g = [g_1^\top, \dots, g_m^\top]^\top, \quad (2.1)$$

we obtain the linear system:

$$Af = g - \epsilon,$$

where ϵ is the unknown noise. Since the size of matrix A and A^\top are huge for the cryo-EM SPM problem, it is not efficient to save the matrix in the computer's memory. In practice, we only compute and save Af and $A^\top g$. Figure 1 shows a 2D example for computing Af and $A^\top g$. Suppose that l is a line with a given projection direction coming across the map f and intersecting it with some pixels in f . We simply sum these pixel values to obtain the discrete

approximation of X-ray transform, as Figure 1 (a) shows. We loop all the directions and lines to obtain Af . In order to compute $u = A^\top g$, for each pixel u_i of u , we sum these pixel values of g whose back-projection directions come across u_i , as shown in Figure 1 (b). We loop all the pixels in u_i to obtain u .

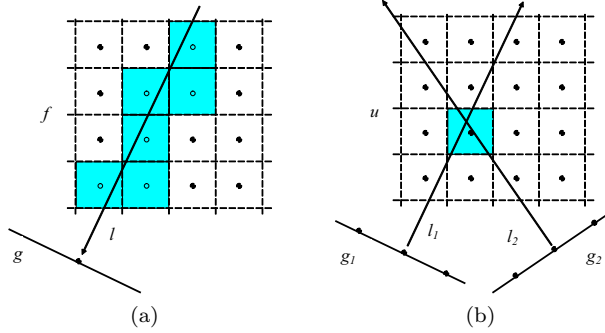


Figure 1. (a) Discretized 2D X-ray transform; (b) Discretized 2D back projection.

In order to reconstruct a 3D density map from its 2D cryo-EM SPM images and refine the Euler angles, we propose the following minimization problem:

$$\min_{\Lambda, f} E(f, \Lambda) = \frac{\kappa}{2} \sum_{i=1}^m \|P_i(\alpha_i)f - g_i\|_2^2 + \|\text{diag}(\lambda)Wf\|_1, \quad (2.2)$$

s.t. $\alpha_i \in \Omega_i, i = 1, \dots, m,$

where $\kappa > 0, \lambda \in \mathbb{R}_+^n, \Lambda = (\alpha_1, \dots, \alpha_m)^\top, \alpha_i = (\theta_i, \phi_i, \psi_i)^\top,$ and $\Omega_i \subset \mathbb{R}^3, i = 1, \dots, m$ are bounded closed convex subsets. W is the orthonormal wavelet decomposition matrix satisfying $W^\top W = I, WW^\top = I.$ Suppose that we have obtained the initial estimations of Λ and $f,$ denoted by Λ^0 and $f^0.$ Our goal is to refine these parameters Λ and f so as to improve the resolution of the 3D map. Hence, we propose to solve the following alternative minimization problems:

$$\alpha_i^{k+1} = \arg \min_{\alpha_i \in \Omega_i} \frac{\kappa}{2} \|P_i(\alpha_i)f^k - g_i\|_2^2, \quad i = 1, \dots, m; \quad (2.3)$$

$$f^{k+1} = \arg \min_f \frac{\kappa}{2} \sum_{i=1}^m \|P_i(\alpha_i^{k+1})f - g_i\|_2^2 + \|\text{diag}(\lambda)Wf\|_1. \quad (2.4)$$

The subproblem (2.3) is a nonlinear least square problem and can be solved using the Levenberg–Marquardt algorithm. Let $F_i^k(\alpha_i) := P_i(\alpha_i)f^k - g_i \in \mathbb{R}^{n^2},$ matrix $J_i^k(\alpha_i) \in \mathbb{R}^{n^2 \times 3}$ is the Jacobian matrix of $F_i^k(\alpha_i)$ defined by

$$J_i^k(\alpha_i) = \begin{pmatrix} \frac{\partial F_{i,1}^k}{\partial \theta_i} & \frac{\partial F_{i,1}^k}{\partial \phi_i} & \frac{\partial F_{i,1}^k}{\partial \psi_i} \\ \vdots & \ddots & \vdots \\ \frac{\partial F_{i,n^2}^k}{\partial \theta_i} & \frac{\partial F_{i,n^2}^k}{\partial \phi_i} & \frac{\partial F_{i,n^2}^k}{\partial \psi_i} \end{pmatrix}.$$

We consider the linearized problem of (2.3) at the point α_i^k

$$s_i^k = \arg \min_{s_i} \frac{1}{2} \|F_i^k(\alpha_i^k) + J_i^k(\alpha_i^k) s_i\|_2^2.$$

The Levenberg–Marquardt algorithm gives

$$s_i^k = -[J_i^k(\alpha_i^k)^\top J_i^k(\alpha_i^k) + \mu_i^k I]^{-1} J_i^k(\alpha_i^k)^\top F_i^k(\alpha_i^k),$$

and the updating scheme of α_i is given by

$$\alpha_i^{k+1} = \alpha_i^k - \sigma_i^k [J_i^k(\alpha_i^k)^\top J_i^k(\alpha_i^k) + \mu_i^k I]^{-1} J_i^k(\alpha_i^k)^\top F_i^k(\alpha_i^k).$$

The subproblem (2.4) can be solved by the iterative soft-thresholding algorithm:

$$f^{k+1} = W^\top T_{\lambda/\kappa} W \left(f^k - \kappa \sigma_f^k \sum_{i=1}^m P_i(\alpha_i^{k+1})^\top F_i^k(\alpha_i^{k+1}) \right), \tag{2.5}$$

where $T_{\lambda/\kappa}$ is defined by

$$T_{\lambda/\kappa}([u_1, u_2, \dots, u_{n^3}]^\top) = [t_{\lambda_1/\kappa}(u_1), t_{\lambda_2/\kappa}(u_2), \dots, t_{\lambda_{n^3}/\kappa}(u_{n^3})]^\top$$

with the soft-thresholding operator $t_{\lambda_i/\kappa}(u_i) = \text{sgn}(u_i) \max(|u_i| - \lambda_i/\kappa, 0)$. Using (2.1) the iteration scheme (2.5) can be reformulated as

$$f^{k+1} = W^\top T_{\lambda/\kappa} W (f^k - \kappa \sigma_f^k (A^{k+1})^\top (A^{k+1} f^k - g)).$$

The stepsizes σ_i^k and σ_f^k are chosen using the following Armijo rule.

DEFINITION 1. Armijo rule [1]. Given the descent direction d^k of function $E(x)$, s , β and ρ with $s > 0, 0 < \beta < 1$, and $0 < \rho < 1$, choosing m_k as the first nonnegative integer m satisfying

$$E(x^k) - E(x^k + \beta^m s d^k) \geq -\rho \beta^m s \nabla E(x^k)^\top d^k,$$

then set the stepsize $\sigma_k = \beta^{m_k} s$.

Then the algorithm solving the orientation refinement problem (2.2) is proposed as follows.

Algorithm 1 Given $\kappa > 0, 0 < \rho < 1, s > 0, 0 < \beta < 1, \alpha_i^0 \in \Omega_i, \mu_i^0 \geq 0, i = 1, \dots, m$ and $f^0 \in \mathbb{R}^{n^3}$. For $k = 0, 1, 2, \dots$,

1. for $i = 1, \dots, m$

(1) $s_i^k = -[J_i^k(\alpha_i^k)^\top J_i^k(\alpha_i^k) + \mu_i^k I]^{-1} J_i^k(\alpha_i^k)^\top F_i^k(\alpha_i^k).$

(2) Choose a stepsize $\sigma_i^k = \beta^{m_k} s$ satisfying the Armijo rule

$$\|F_i^k(\alpha_i^k + \sigma_i^k s_i^k)\|^2 \leq \|F_i^k(\alpha_i^k)\|^2 + \rho \sigma_i^k [J_i^k(\alpha_i^k)^\top F_i^k(\alpha_i^k)]^\top s_i^k. \tag{2.6}$$

(3) If $\alpha_i^k + \sigma_i^k s_i^k / \beta \notin \Omega_i$, then let $\mu_i^{k+1} = 4\mu_i^k$, $\alpha_i^{k+1} = \alpha_i^k$, $i = i + 1$, go to (1).

(4) $\alpha_i^{k+1} = \alpha_i^k + \sigma_i^k s_i^k$, $\mu_i^{k+1} = 0.5\mu_i^k$, $i = i + 1$.

2. $d_f^k = -\kappa(A^{k+1})^\top (A^{k+1} f^k - g)$

(1) Choose a stepsize $\sigma_f^k > 0$ satisfying the Armijo rule

$$E(W^\top T_{\lambda/\kappa} W (f^k + \sigma_f^k d_f^k), A^{k+1}) \leq E(f^k, A^{k+1}) - \rho \sigma_f^k d_f^k{}^\top d_f^k. \tag{2.7}$$

3. $f^{k+1} = W^\top T_{\lambda/\kappa} W (f^k + \sigma_f^k d_f^k)$.

In the implement of the Algorithm 1, the jacobian matrix $J_i^k(\alpha_i)$ is approximately calculated by employing the finite difference scheme. For example, in order to compute $\frac{\partial F_{i,1}}{\partial \theta_i}$, we have

$$\frac{\partial F_{i,1}}{\partial \theta_i} \approx \frac{F_{i,1}(\theta_i^k + h^k, \phi_i^k, \psi_i^k) - F_{i,1}(\theta_i^k, \phi_i^k, \psi_i^k)}{h^k}.$$

3 Convergence Analysis

In this section, we analyze the convergence of the proposed algorithm. The result is given by the following theorem.

Theorem 1. Let $\Omega_i \subset \mathbb{R}^3$, $i = 1, \dots, m$ be bounded closed convex subsets, and $\{A^k{}^\top A^k\}$ be a nonsingular matrix sequence for $\alpha_i \in \Omega_i, i = 1, \dots, m$ and uniformly bounded. Then we have

(1) the sequences $\{\alpha_i^k\}, i = 1, \dots, m$ and $\{f^k\}$ generated by Algorithm 1 have convergent subsequences, denoted by $\{\alpha_i^k\}_{\mathcal{K}}, i = 1, \dots, m$, and $\{f^k\}_{\mathcal{K}}$, where $\mathcal{K} \subseteq \{0, 1, \dots\}$.

(2) Let $\lim_{k \in \mathcal{K}} \alpha_i^k = \alpha_i^*, i = 1, \dots, m; \lim_{k \in \mathcal{K}} f^k = f^*$. If there exists two positive scalars c_1, c_2 and $\mu_i^k > 0$, such that

$$c_1 \|x\|^2 \leq x^\top [J_i^k(\alpha_i^k)^\top J_i^k(\alpha_i^k) + \mu_i^k I]^{-1} x \leq c_2 \|x\|^2, \quad \forall x \in \mathbb{R}^3, i = 1, \dots, m \tag{3.1}$$

for all k , then $(f^*, \alpha_1^*, \dots, \alpha_m^*)$ is a stationary point.

Proof. (1). For $i = 1, 2, \dots, m$, since $\{\alpha_i^k\} \subset \Omega_i$, then there exists a convergent subsequence $\{\alpha_i^k\}_{\mathcal{K}_1} (\mathcal{K}_1 \subseteq \{0, 1, \dots\})$.

Taking the spectral norm of the matrix, we have

$$\|I\| = 1, \quad \|W\|^2 = \|W^\top W\| = 1, \quad \|W\| = \|W^\top\| = 1,$$

and according to the result in [7], T_λ is nonexpansive, then $\forall u, v \in \mathbb{R}^{n^3}$,

$$\begin{aligned} \|W^\top T_\lambda W u - W^\top T_\lambda W v\| &= \|W^\top (T_\lambda W u - T_\lambda W v)\| \\ &\leq \|W^\top\| \|T_\lambda W u - T_\lambda W v\| \\ &\leq \|W u - W v\| = \|u - v\|. \end{aligned}$$

By taking $v = 0$, we have $\|W^\top T_\lambda W u\| \leq \|u\|$.

Since the matrix $A^k \top A^k$ is nonsingular and uniformly bounded, there exist $\sigma_M, \sigma_m > 0$ such that $0 < \|A^k\| < \sigma_M$, and for all $k = 1, \dots$, the minimal singular value $\sigma_{\min}(A^k) > \sigma_m$. Take $\frac{1}{2\sigma_M^2} < \kappa < \frac{1}{\sigma_M^2}$, then

$$0 < \|I - \kappa A^k \top A^k\| < 1 - 0.5\sigma_m^2/\sigma_M^2.$$

Denote $\omega = 1 - 0.5\sigma_m^2/\sigma_M^2$, then

$$\begin{aligned} \|f^{k+1}\| &= \|W \top T_{\lambda/\kappa} W [(I - \kappa A^k \top A^k) f^k + \kappa A^k \top g]\| \\ &\leq \|(I - \kappa A^k \top A^k) f^k + \kappa A^k \top g\| \leq \omega \|f^k\| + \kappa \sigma_M \|g\| \\ &\leq \omega^{k+1} \|f^0\| + \kappa \sigma_M \|g\| \frac{1 - \omega^{k+1}}{1 - \omega} \leq \|f^0\| + \frac{\|g\|}{\sigma_M(1 - \omega)}. \end{aligned}$$

Therefore, there exists a convergent subsequence $\{f^k\}_{k \subseteq \mathcal{K}_1}$.

(2). From the left inequality of (3.1) we can deduce that $[J_i^k(\alpha_i^k) \top J_i^k(\alpha_i^k) + \mu_i^k I]^{-1}$ is positive definite, and $[J_i^k(\alpha_i^k) \top F_i^k(\alpha_i^k)] \top s_i^k < 0$, the Armijo rule (2.6) implies that

$$\|F_i^k(\alpha_i^k + \sigma_i^k s_i^k)\| \leq \|F_i^k(\alpha_i^k)\|,$$

then for $i = 1, \dots, m$ we have

$$E(f^k, \alpha_1^{k+1}, \dots, \alpha_i^{k+1}, \alpha_{i+1}^k, \dots, \alpha_m^k) \leq E(f^k, \alpha_1^{k+1}, \dots, \alpha_i^k, \alpha_{i+1}^k, \dots, \alpha_m^k). \tag{3.2}$$

The Armijo rule (2.7) implies that

$$E(f^{k+1}, \alpha_1^{k+1}, \dots, \alpha_m^{k+1}) \leq E(f^k, \alpha_1^{k+1}, \dots, \alpha_m^{k+1}). \tag{3.3}$$

Using (3.2) and (3.3), we obtain

$$E(f^{k+1}, \alpha_1^{k+1}, \dots, \alpha_m^{k+1}) \leq E(f^k, \alpha_1^k, \dots, \alpha_m^k).$$

Hence $\{E(f^k, \alpha_1^k, \dots, \alpha_m^k)\}$ is nonincreasing. Since $\{(f^k, \alpha_1^k, \dots, \alpha_m^k)\}_{k \in \mathcal{K}}$ converges to $(f^*, \alpha_1^*, \dots, \alpha_m^*)$ and E is continuous, we have

$$\lim_{\substack{k \rightarrow \infty \\ k \in \mathcal{K}}} E(f^k, \alpha_1^k, \dots, \alpha_m^k) = E(f^*, \alpha_1^*, \dots, \alpha_m^*).$$

Then from (2.6) and (2.7) we have

$$\{\sigma_i^k [J_i^k(\alpha_i^k) \top F_i^k(\alpha_i^k)] \top s_i^k\} \rightarrow 0, \quad i = 1, \dots, m, \tag{3.4}$$

$$\{\sigma_f^k d_f^k \top d_f^k\} \rightarrow 0. \tag{3.5}$$

Suppose that $\{s_i^k\}_{k \in \mathcal{K}} \not\rightarrow 0$ and $\{d_f^k\}_{k \in \mathcal{K}} \not\rightarrow 0$. By possibly restricting to subsequences of $\{s_i^k\}_{k \in \mathcal{K}}$ and $\{d_f^k\}_{k \in \mathcal{K}}$, we assume that for some $\delta > 0$, $\|s_i^k\| \geq \delta$, $\|d_f^k\| \geq \delta$, for all $k \in \mathcal{K}$. Then, from (3.4) and (3.5), we have $\{\sigma_i^k\}_{k \in \mathcal{K}} \rightarrow 0$, $i = 1, \dots, m$ and $\{\sigma_f^k\}_{k \in \mathcal{K}} \rightarrow 0$. By the Definition 1 of the Armijo rule, and the Algorithm 1, we have for $i = 1, \dots, m$

$$\begin{aligned} &\|F_i^k(\alpha_i^k)\|^2 - \|F_i^k(\alpha_i^k + (\sigma_i^k/\beta) s_i^k)\|^2 \\ &< -\rho(\sigma_i^k/\beta) [J_i^k(\alpha_i^k) \top F_i^k(\alpha_i^k)] \top s_i^k, \quad \forall k \in \mathcal{K}, \end{aligned} \tag{3.6}$$

where $\alpha_i^k + (\sigma_i^k/\beta)s_i^k \in \Omega_i$. Denote $p_i^k = s_i^k/\|s_i^k\|$, $\bar{\sigma}_i^k = \sigma_i^k\|s_i^k\|/\beta$, then from (3.6) we have

$$\frac{\|F_i^k(\alpha_i^k)\|^2 - \|F_i^k(\alpha_i^k + \bar{\sigma}_i^k p_i^k)\|^2}{\bar{\sigma}_i^k} < -\rho [J_i^k(\alpha_i^k)^\top F_i^k(\alpha_i^k)]^\top p_i^k, \quad \forall k \in \mathcal{K}.$$

By using the mean value theorem, this relation becomes

$$- [J_i^k(\alpha_i^k + \tilde{\sigma}_i^k p_i^k)^\top F_i^k(\alpha_i^k + \tilde{\sigma}_i^k p_i^k)]^\top p_i^k < -\rho [J_i^k(\alpha_i^k)^\top F_i^k(\alpha_i^k)]^\top p_i^k, \quad \forall k \in \mathcal{K}, \tag{3.7}$$

where $\tilde{\sigma}_i^k \in [0, \bar{\sigma}_i^k]$. From the right inequality of (3.1) we can deduce that $\|[J_i^k(\alpha_i^k)^\top J_i^k(\alpha_i^k) + \mu_i^k I]^{-1}\| \leq c_2$, then

$$\begin{aligned} \sigma_k \|s_i^k\| &\leq \sigma_k \|[J_i^k(\alpha_i^k)^\top J_i^k(\alpha_i^k) + \mu_i^k I]^{-1}\| \| [J_i^k(\alpha_i^k)^\top F_i^k(\alpha_i^k)] \| \\ &\leq \sqrt{\sigma_k} \|[J_i^k(\alpha_i^k)^\top J_i^k(\alpha_i^k) + \mu_i^k I]^{-1}\| \left(\frac{\| \sigma_k [J_i^k(\alpha_i^k)^\top F_i^k(\alpha_i^k)]^\top s_i^k \|}{c_1} \right)^{1/2}. \end{aligned}$$

Using (3.4) we have $\{\bar{\sigma}_i^k\}_{\mathcal{K}} \rightarrow 0$, and since $\|p_i^k\| = 1, \forall k \in \mathcal{K}$, there exists a subsequence $\{p_i^k\}_{\bar{\mathcal{K}} \subseteq \mathcal{K}}$ such that

$$\{p_i^k\}_{\bar{\mathcal{K}}} \rightarrow p_i^*, \quad \|p_i^*\| = 1.$$

Taking limits in the equation (3.7) we obtain

$$- [J_i(\alpha_i^*)^\top F_i(\alpha_i^*)]^\top p_i^* \leq -\rho [J_i(\alpha_i^*)^\top F_i(\alpha_i^*)]^\top p_i^*,$$

or

$$0 \leq (1 - \rho) [J_i(\alpha_i^*)^\top F_i(\alpha_i^*)]^\top p_i^*.$$

Since $0 < \rho < 1$, it follows that

$$[J_i(\alpha_i^*)^\top F_i(\alpha_i^*)]^\top p_i^* \geq 0. \tag{3.8}$$

On the other hand,

$$[J_i^k(\alpha_i^k)^\top F_i^k(\alpha_i^k)]^\top p_i^k = \frac{[J_i^k(\alpha_i^k)^\top F_i^k(\alpha_i^k)]^\top s_i^k}{\|s_i^k\|} < 0.$$

By taking the limits as $k \in \bar{\mathcal{K}}, k \rightarrow \infty$,

$$[J_i(\alpha_i^*)^\top F_i(\alpha_i^*)]^\top p_i^* < 0,$$

which arrives at a contradiction. Hence, we have $\{s_i^k\}_{\mathcal{K}} \rightarrow 0$, and it follows that $J_i(\alpha_i^*)^\top F_i(\alpha_i^*) = 0$ for $i = 1, \dots, m$.

From the boundedness of $\|A^{k+1}\|$ and $\|A^{k+1}f^k - g\|$ we can deduce that d_f^k is bounded. And then using the Armijo rule (2.7) we can prove that $d_f^* = 0$ similarly. Hence, $(f^*, \alpha_1^*, \dots, \alpha_m^*)$ is a stationary point of $E(f, \Lambda)$. Part (2) of the theorem is proved. \square

Based on the discretization method of the X-ray transform we used, the matrix P_i is full row rank since no two lines can go through the same set of voxels. For the cryo-EM SPM problem, the number of orientations is normally far more than the number of images, that is $m \gg n$. When the orientations of the images are distributed even uniformly on the unit sphere, $A^{k\top} A^k$ is nonsingular. The uniformly boundedness of $A^{k\top} A^k$ can be satisfied if A^k is uniformly bounded. In fact, from the discretization method of the X-ray transform we proposed, the elements of A^k are 1 or 0. Therefore, for m orientations and n images, the Frobenius norm of $\|A^k\|_F$ satisfies $\|A^k\|_F \leq \sqrt{mn}^3$, which means A^k is uniformly bounded. Finally, the condition (3.1) can be satisfied by Algorithm 1 by adjusting the parameter μ_i^k at each iteration.

4 Numerical Experiments

In this experiment, we simulate the cryo-EM SPM particle images using the E. coli ribosome crystal structure 3I1M.pdb¹ and 3I1N.pdb². A 3D density map of E. coli ribosome with pixel size 2.82 Å and volume size $131 \times 131 \times 131$ is generated by first combining the two crystal structure into one and then filtering it using Gaussian convolution. After that, 5000 simulated particle images with size 131×131 pixels are generated from this 3D density map using randomly orientations, part of which are shown in Figure 2.

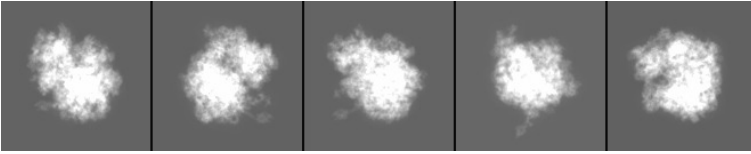


Figure 2. Simulated E. coli ribosome cryo-EM SPM particle images.

Each orientation for one image is saved as three Euler angles (θ, ϕ, ψ) . In order to construct the dataset for the proposed algorithm, we disturb the set of Euler angles to produce inaccurate Euler angles $(\tilde{\theta}, \tilde{\phi}, \tilde{\psi})$, that is $|\tilde{\theta}_i - \theta_i| < \delta$, $|\tilde{\phi}_i - \phi_i| < \delta$ and $|\tilde{\psi}_i - \psi_i| < \delta$ for $i = 1, \dots, 5000$. We takes $\delta = 1^\circ, 3^\circ, 9^\circ, 21^\circ$ and 39° respectively to obtain five sets of inaccurate Euler angles Λ_i^0 , $i = 1, \dots, 5$ and these five sets of Euler angles are used to reconstruct five errored 3D maps f_i^0 , $i = 1, \dots, 5$. Each pair of (Λ_i^0, f_i^0) are used to test the proposed algorithm. The proposed algorithm is implemented using Haar wavelet orthonormal base, parallelized using MPI (message passing interface), and run on the computer cluster³ with totally 100 processes. These test results are shown in Table 1. The mean square error (MSE) is used to evaluate the algorithm which defines as follows

$$\text{MSE}(A, A^k) = \frac{1}{m} \|A - A^k\|_F,$$

¹ <http://www.rcsb.org/pdb/explore.do?structureId=3i1m>

² <http://www.rcsb.org/pdb/explore.do?structureId=3i1n>

³ Computer cluster "LSSC3" in ICMSEC at CAS with totally 282 nodes and 24 GB memory each

where $\| \cdot \|_F$ is the Frobenius norm, Λ and Λ^k are the correct Euler angles and the refinement results at the iteration k , respectively. Define $\text{InitMSE} = \text{MSE}(\Lambda, \Lambda^0)$ as the initial error.

Table 1. Orientation refinement results for the simulated cryo-EM SPM particle images.

clean image	1°	3°	9°	21°	39°
InitMSE	0.02451	0.0733	0.2213	0.5137	0.9559
MSE	0.01096	0.0169	0.0250	0.0554	0.2408
iterations	30	38	48	48	57

From Table 1 we can conclude that the algorithm improve the errors of the Euler angles, even for the big angles errors 39°. The output reconstructions are shown in Figure 3, from which we can see that the resolutions of the 3D maps are improved apparently by the proposed algorithm.

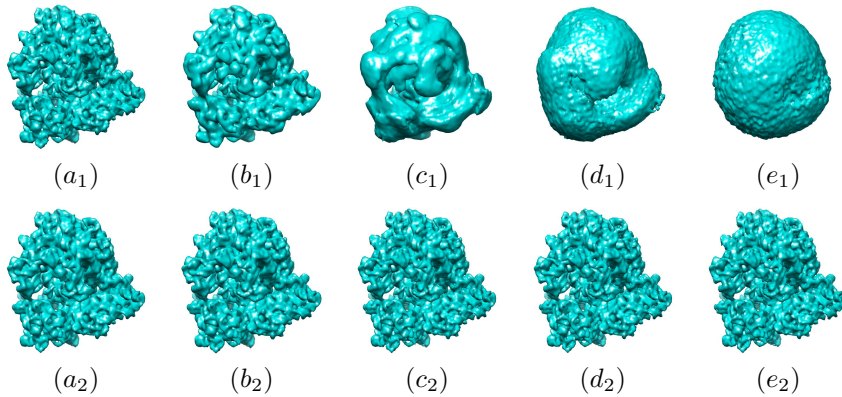


Figure 3. The comparisons of the initial maps (first row) and the refinement maps (second row) using the proposed algorithm. The maps from column (a) to column (e) show the cases for 1°, 3°, 9°, 21° and 39° respectively.

Since cryo-EM SPM particle images have extremely low SNR, in our second experiment, Gaussian white noise is added on each image to obtain noisy image with $\text{SNR} = 0.1$. Part of these simulated noisy particle images are shown in Figure 4.

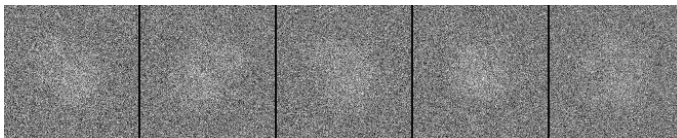
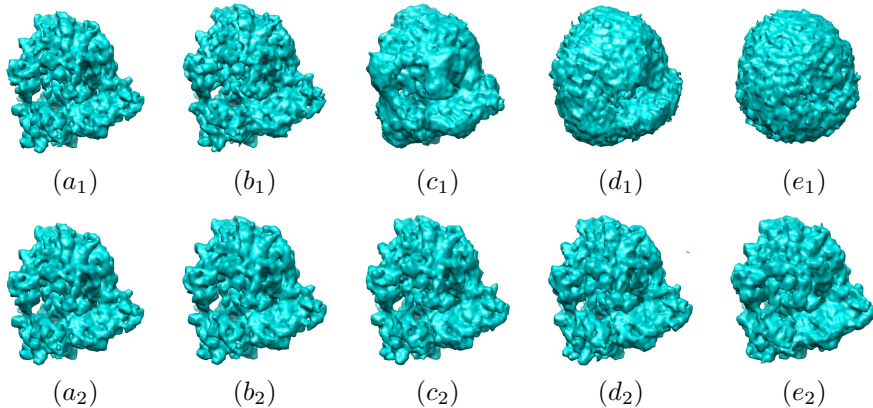


Figure 4. Simulated E. coli ribosome cryo-EM SPM particle images with $\text{SNR} = 0.1$.

We run the proposed algorithm for the five pairs of initial values (Λ_i^0, f_i^0) , $i = 1, \dots, 5$ again for the noisy images. Table 2 gives the results. We can see that

Table 2. Orientation refinement results for the simulated noisy particle images.

SNR= 0.1	1°	3°	9°	21°	39°
InitMSE	0.02451	0.0733	0.2213	0.5137	0.9559
MSE	0.02384	0.0550	0.1007	0.1911	0.5258
iterations	12	15	33	42	49

**Figure 5.** The comparisons of the initial maps (first row) and the refinement maps (second row) using the proposed algorithm for the noisy images. The maps from column (a) to column (e) show the cases for 1°, 3°, 9°, 21° and 39° respectively.

the errors can still be improved even for the worst case 39°. The reconstructed maps for the refinement Euler angles are given in Figure 5. We can conclude that for the noisy images, the reconstructed maps using the proposed algorithm have obtained improved resolutions compared with the initial maps.

5 Conclusions

In this paper we have proposed the alternative iteration orientation refinement method combining the Levenberg–Marquardt algorithm and wavelet orthonormal bases based iterative soft-thresholding. The convergence analysis and numerical experiments show that the proposed algorithm is effective and efficient for the simulated cryo-EM SPM particle images. For the true cryo-EM SPM experimental particle images, since the noise in the images is a combination of several different noise sources coming from the imaging process, the algorithm will be improved in the future to deal with the non-Gaussian noise images.

Acknowledgments

The authors would like to thank the reviewers for careful reading and helpful comments. The work of Zhucui Jing and Ming Li are partially supported by the research grant 11101401 from NSFC for Youth.

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